



# Optimal control problems with sparsity constraints in image processing

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# Outline

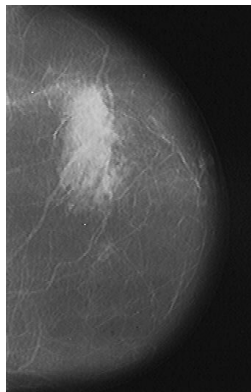
- 1 Introduction: Optimize presentation of mammography images
- 2 Modelling: Optimal control of PDEs
- 3 Algorithms: Generalized conditional gradient methods and the method of surrogate functionals
- 4 Application



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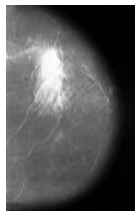
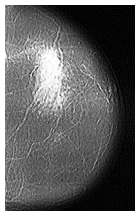
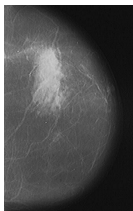
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# Mammography screening



- Examination of X-ray scans
- Several thousand scans per year
- Mammographie Projekt Bremen

## The examination: a sweep across scales



$y_0$  original     $y_f$  fine scales     $y_c$  coarse scale

Display:  $y(t)$ ,  $t \in [0, 1]$ , with

$$y(0) = y_0, \quad y(.5) = y_f, \quad y(1) = y_c$$

Easier: Just two images  $y_0$  and  $y^*$  with

$$y(0) = y_0, \quad y(1) = y^*$$



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- 2 **Modelling: Optimal control of PDEs**
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# Use an optimal controlled PDE for interpolation

## An initial value problem

$$\begin{aligned}y_t &= D(y) \\ y(0) &= y_0\end{aligned}$$

But we desire:  $y(1) \stackrel{!}{=} y^*$

## An optimal controlled initial value problem

$$\begin{aligned}&\text{Minimize } \int |y(1) - y^*|^2 dx + \alpha \|u\|^2 \\ &\text{subject to } y_t = D(u, y), \quad y(0) = y_0\end{aligned}$$

# What PDE to use for modelling the sweep?

Source term

allow contrast changes  
allow formation of details

$$y_t - \operatorname{div}(P \nabla y) = u$$

Diffusion tensor

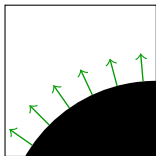
keep edges sharp,  
allow movement of edges  
remove textures

# One particular model: Source term and diffusion tensor

$$\min_{u, P, y} \int |y(1) - y^*|^2 dx + \alpha_u \|u\|^2 + \alpha_P \Phi_P(P)$$

where  $y$  solves

$$\begin{aligned} y_t - \operatorname{div}(P \nabla y) &= u \\ \partial_{\nu_P} y &= 0 \\ y(0, x) &= y_0(x). \end{aligned}$$



with diffusion tensor

$$P = (I - \sigma(|p|)) \frac{p}{|p|} \otimes \frac{p}{|p|}$$

( $|p| = 1$ : projection on  $p^\perp$ )

(K. Bredies)



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# From optimal control to inverse problems

## The control-to-state operator

$$A : u \xrightarrow{\text{Solve PDE}} y \xrightarrow{\text{restrict to endpoint}} y(1)$$

## The reduced cost functional aka Tikhonov regularization

With the help of the control to state mapping

$$\int |y(1) - y^*|^2 dx + \alpha \|u\|^2$$

becomes

$$\|Au - y^*\|^2 + \alpha \|u\|^2.$$



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Make the problem  $Au = y^*$  well-posed.

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## Regularization:

Make the problem  $Au = y^*$  well-posed.

## Constraint:

Solve  $Au = y^*$  while  $u$  has further properties.



# Tool from constraint optimization: the conditional gradient method

$$\min_{u \in C} F(u) \quad \text{by}$$

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$$\min_{u \in C} F(u) \quad \text{by} \quad \begin{array}{l} \text{1} \text{ directional derivative } v_n \text{ by} \\ \min_{v \in C} \langle F'(u_n) | v \rangle \end{array}$$

2 step size  $s_n$  by

$$\min_{s \in [0,1]} F(u_n + s(v_n - u_n))$$

3 update

Dunn, 1980

$$u_{n+1} = u_n + s_n(v_n - u_n)$$

# Tool from constraint optimization: the conditional gradient method

$\min F(u) + \Phi(u)$  by

1 directional derivative  $v_n$  by

$$\min \langle F'(u_n) | v \rangle + \Phi(u)$$

2 step size  $s_n$  by

$$\min_{s \in [0,1]} (F + \Phi)(u_n + s(v_n - u_n))$$

3 update

K. Bredies

$$u_{n+1} = u_n + s_n(v_n - u_n)$$

# The generalized conditional gradient method converges

## Theorem

$\Phi$  proper, convex, lsc.

$F$  continuously differentiable,  $F + \Phi$  coercive and

$$E_t = \{\Phi(u) \leq t\} \text{ compact for every } t.$$

Then: convergence to a stationary point of  $F + \Phi$ .

*K. Bredies, D. L., P. Maass, 2005*

Remark:  $F$  need not to be convex.

# The generalized conditional gradient method is iterated shrinkage

## Proposition

The minimization of

$$\|Au - y^*\|^2 + \alpha \sum w_j |\langle u | \psi_j \rangle|^p$$

with the generalized conditional gradient method for

$$F(u) = \|Au - y^*\|^2 - \|u\|^2, \quad \Phi(u) = \|u\|^2 + \alpha \sum w_j |\langle u | \psi_j \rangle|^p$$

gives the iteration

$$u_{n+1} = \mathbf{S}_{\alpha w_j, p}(u_n - A^*(Au_n - y^*))$$

where  $\mathbf{S}$  is an elementwise shrinkage operation.

# Remarks on iterated shrinkage

## Remarks

- The iterated shrinkage is also motivated by the methods of surrogate functionals (Daubechies, Defries, DeMol, 2004).
- The above proposition also applies to nonlinear operators  $A$ :

$$\min \|A(u) - y^*\|^2 + \alpha \sum w_j |\langle u | \psi_j \rangle|^p$$

gives

$$u_{n+1} = \mathbf{S}_{\alpha w_j, p}(u_n - A(u_n)^*(A(u_n) - y^*))$$



# Brief sketch of the surrogate method

$$\|Au - y^*\|^2 + \alpha \sum w_j |\langle u | \psi_j \rangle|^p$$



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Decouple  $A$  and  $|\cdot|^p$

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$$\begin{aligned} \|Au - y^*\|^2 + \alpha \sum w_j |\langle u | \psi_j \rangle|^p + (\|u - a\|^2 - \|Au - Aa\|^2) \\ = J(u, a) \end{aligned}$$

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Decouple  $A$  and  $|\cdot|^p$   
alternate minimization for  $u, a$

### Theorem

$$u_{n+1} = \operatorname{argmin}_u J(u, u_n) = \mathbf{S}_{\alpha w_j, p}(u_n - A^*(Au_n - y^*))$$

*converges strongly to a minimizer of  $\|Au - y^*\|^2 + \alpha \sum w_j |\langle u | \psi_j \rangle|^p$ .  
Daubechies, Defries, De Mol, 2004.*



# Trying to get “extremely sparse”

$$\Phi(u) = \#\{\langle u|\psi_j\rangle \neq 0\}$$



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For  $p < 1$  the problem is non-convex.

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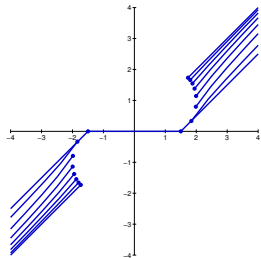
$$\Phi(u) = \sum w_j |\langle u | \psi_j \rangle|^p$$

For  $p < 1$  the problem is non-convex.  
Special case  $A = I$ :

$$\|u - y^*\|^2 + \alpha \sum w_j |\langle u | \psi_j \rangle|^p$$

has a “unique” minimizer.

$$\begin{aligned} \bar{u} &= \mathbf{S}_{\alpha, w_j, p}(y^*) \\ &= \sum S_{\alpha, w_j, p}(\langle y^* | \psi_j \rangle) \psi_j \end{aligned}$$



# Non-convex penalties in the surrogate method again gives shrinkage

## Proposition ( $p = 0$ )

- The iteration

$$u_{n+1} = \operatorname{argmin}_u \|Au - y^*\|^2 + \alpha \#\{\langle u | \psi_j \rangle \neq 0\} \\ + (\|u - u_n\|^2 - \|Au - Au_n\|^2)$$

gives the iterated hard shrinkage

$$u_{n+1} = \mathbf{S}_{\sqrt{2\alpha}}(u_n - A^*(Au_n - y^*)).$$

- If the sequence  $u_n$  converges, it converges to a minimizer of  $\|Au - y^*\|^2 + \alpha \#\{\langle u | \psi_j \rangle \neq 0\}$ .



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# Sparse reconstruction under the presence of noise

$(\psi_j)$ : Two ONBs (Haar wavelet packet basis + spike basis)

$\bar{y}$ : finite linear combination of  $\psi_j$ 's

$y^*$ :  $\bar{y}$  + noise

$Hu = \sum u_j \psi_j$ : Reconstruction operator.

Try to recover the sparse representation of  $\bar{y}$  from  $y^*$ .

minimize  $\|Hu - y^*\|^2 + \alpha \sum |u_j|^p$



# Sparse reconstruction under the presence of noise

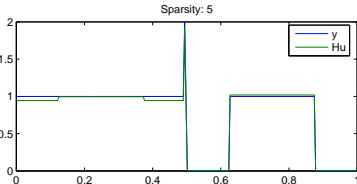
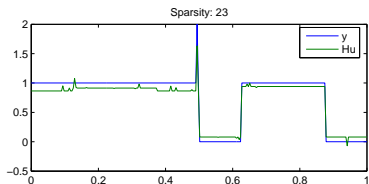
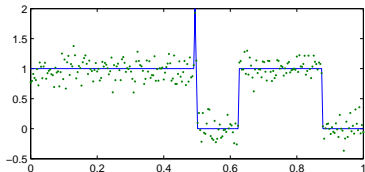
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# Summary

- Optimization of the presentation of mammography images by optimal control of PDEs
- The generalized conditional gradient method converges even for non-convex functionals
- The method of surrogate functionals is a generalized conditional gradient descent
- Non-convex sparsity constraints seem to be handable by the method of surrogate functionals